Inference of Latent Neural Field Intensities from Spatiotemporal **Point-Process Observations**

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1. 3-State model for waves in excitable medium 3.

Recover latent fields from spikes: Bayesian filtering

Three-state neural field model, Buice & Cowan '09 (1): complex wave patterns without inhibitory cells.



Figure 1. Quiescent-Active-Refractory (QAR) model of neural waves. The Q-A-R states (1) correspond to the Critical-Active-Stable retinal wave model of Hennig et al. '09 (2) and the Susceptible-Infected-Recovered model in epidemiology.

3 states

2.

5.

4 rate parameters

- ρ_q Spontaneous spiking; Q to A $\square \rightarrow \blacksquare$ • **Q** Quiescent
- ρ_a A to R transition $\blacksquare \rightarrow \blacksquare$ • A Active
- $\rho_r \ \mathsf{R}$ to Q transition $\blacksquare \rightarrow \blacksquare$ • **R** Refractory
 - ρ_e Active cells excite Quiescent \blacksquare \rightarrow \blacksquare

Mean-field dynamics (exclude spontaneous $Q \rightarrow A$)



Figure 3. Hidden Markov model for latent neural fields. For all time-points T, state transition parameters $\theta = (\rho_q, \rho_a, \rho_r, \rho_e, \sigma)$ dictate the evolution of a multivariate Gaussian model μ , Σ of latent fields Q, A, R. Observation model β is a linear map with adjustable gain and threshold, and reflects how field A couples to firing intensity λ . Pointprocess observations (spikes) y are Poisson with intensity λ .

Predict state:

- Multivariate Gaussian state-space model $\mu = (Q, A, R)$, covariance Σ
- Integrate forward μ mean-field equations
- Covariance Σ evolves according to the system Jacobian J
- Similar to continuous-time extended Kalman filter $\dot{\Sigma} = J\Sigma + \Sigma J^T + \Sigma_{\text{noise}}$

Measurement:

- Refine estimate using spiking observations
- Spikes: Poisson events with intensity $\lambda = mA + b$
- Posterior is proportional to product of predicted state and data likelihood
- Laplace approximation (gradient descent; constrain to positive field intensities)



0

Bipolar and amacrine cells (generate waves)

$$\dot{Q} = -
ho_e A Q +
ho_r R$$

 $\dot{A} = -
ho_a A +
ho_e A Q$
 $\dot{R} = -
ho_r R +
ho_a A$

Spontaneous $Q \rightarrow A$ sampled as shot noise (Poisson).

Spatial system

Let fields depend on coordinates (x, y) and define a lateral excitation kernel k with radius σ_i (Nonlocal interactions)

 $k(x,y) \propto \exp\left(-\frac{1}{2}\frac{x^2+y^2}{\sigma_i^2}\right)$



Figure 2. 3-state model can exhibit self-organized wave phenomena. Simulated on a $[0, 1]^2$ unit interval using 20x20 grid, σ =0.04, ρ_a =0.1, ρ_r =10⁻³, $\rho_e=0.4$. Spontaneous excitation rate $\rho_q=0.05$. A finite threshold of 10^{-3} avoids widespread spontaneous excitation. Colors: Quiescent Active Refractory

In practice



Figure 4. Illustration of inner retina and recording setup. Spontaneous retinal waves are generated in a layer of laterally interconnected amacrine cells. These waves activate Retinal Ganglion Cells (RGCs), the output cells of the retina. RGC electrical activity is recorded via a 64×64 multi-electrode array with 50 μ m spacing.

High-density multielectrode array recordings of retinal waves

• 4096-electrode arrays (3)

4.

- Recordings courtesy of the Sernagor lab (4, 5)
- Spontaneous waves during development (6)
- Small events divide retina into refractory patches
- Rare large events sweep across the retina
- Self-organized structure at multiple scales (2)





Figure 5. 4096-electrode array. Left: Array (3). *Right:* Spikes recorded in a single session.



Figure 6. Example wave event, spike histograms in one-second intervals. Mouse retina, postnatal day 11.

Bayesian filtering recovers latent states

Numerically challenging:

• 3 states, 10×10 grid \rightarrow 300-D covariance matrix (4.5k entries)

- Avoid inverses: work with inverse covariance (precision) matrix
- Improve stability: Cholesky factorization, triangular system solvers
- *Regularize* state variance

Performance e.g.:

- 37 s to filter 25 minutes of retinal data, $\Delta t=1 s$, ~40 samples/s
- 10×10 grid; Matlab implementation, 2.9 GHz 8-core Xeon CPU
- Complexity dominated by matrix multiplication

Fluctuations:

- A model of fluctuations is needed to model uncertainty in state estimation
- Use a linear noise approximation of the original discrete system

$$\Sigma_{\text{noise}} = \begin{bmatrix} \rho_e A Q + \rho_r R & -\rho_e A Q & -\rho_r R \\ -\rho_e A Q & \rho_i A + \rho_e A Q & -\rho_i A \\ -\rho_r R & -\rho_i A & \rho_r R + \rho_i A \end{bmatrix}$$



Figure 7. Filtering recovers retinal wave states. Frames shown every 48 seconds; postnatal day 10.

Main points

6.

- Spatiotemporal neural phenomena are complex: excitability, nonlinearity, refractoriness
- Previous spatiotemporal point-process inference procedures unsuitable (simple, linear)
- Three-state neural field model is suitable for inference
- Bayesian filtering recovers latent states, correlation structure, and model likelihood
- Future: optimize for fast parameter inference and apply to basic neuroscience

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